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Helgesson

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[54] **AUTOMATIC FREQUENCY CONTROL SYSTEM FOR DRIVING A LINEAR ACCELERATOR**

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[52] **U.S. Cl.** ..... **328/233;** 315/5.41; 315/39.51; 315/63; 250/492 B

[51] **Int. Cl.**[2] **H05H 9/00**

[58] **Field of Search** ..... 315/5.13, 39.51, 61, 315/63, 5.42, 5.41; 328/233; 313/93; 331/5, 6; 250/492 A, 492 B, 396, 397, 300

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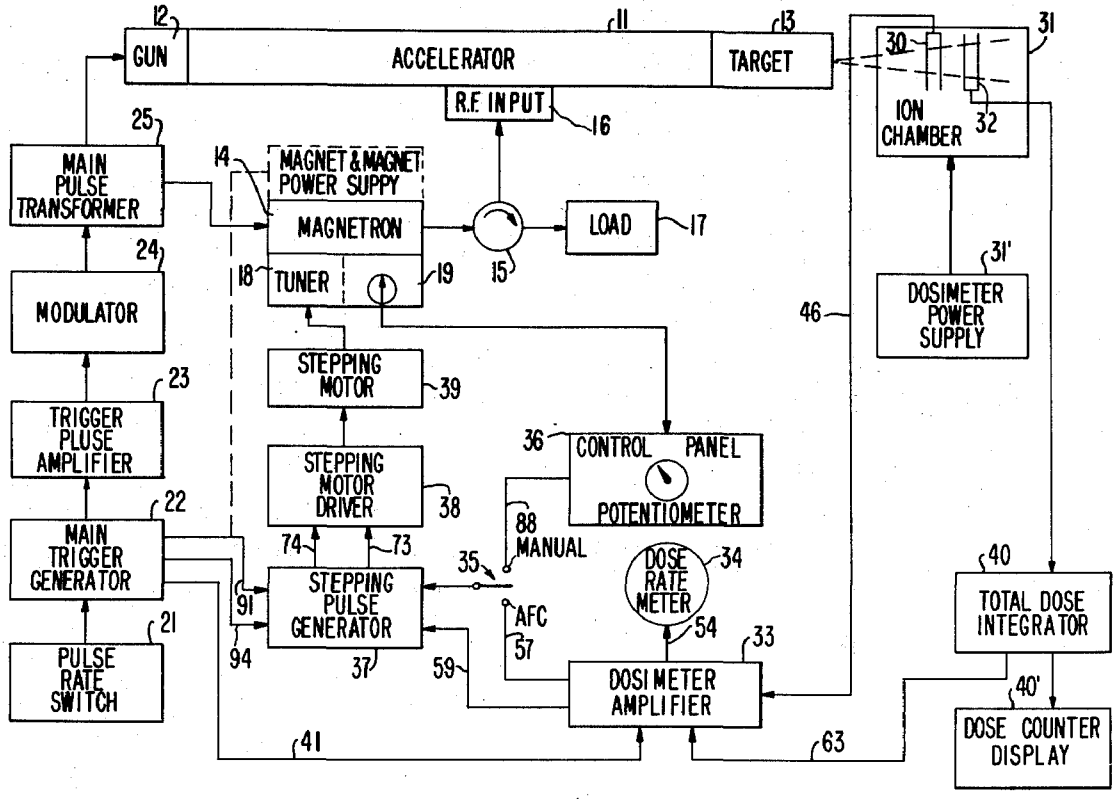
Assistant Examiner—Richard A. Rosenberger
Attorney, Agent, or Firm—Limbach, Limbach & Sutton

[57] **ABSTRACT**

An automatic frequency control system is described for maintaining the drive frequency applied to a linear accelerator to produce maximum particle output from the accelerator. The particle output amplitude is measured and the frequency of the radio frequency source powering the linear accelerator is adjusted to maximize particle output amplitude.

12 Claims, 4 Drawing Figures



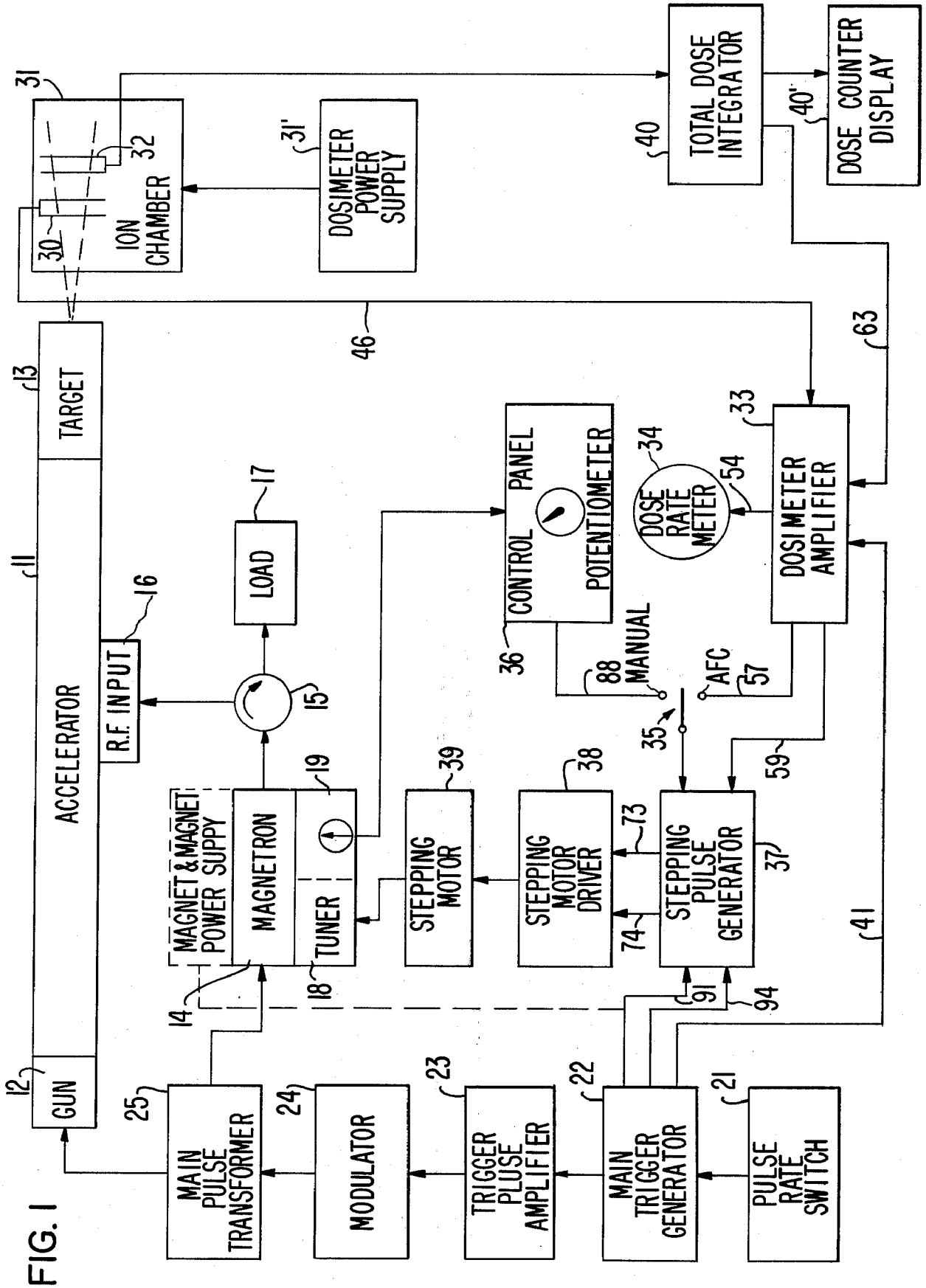

31
32
ION CHAMBER
30
31'
DOSIMETER POWER SUPPLY
40
TOTAL DOSE INTEGRATOR
40'
DOSE COUNTER DISPLAY
46
63
13
TARGET
11
ACCELERATOR
16
R.F. INPUT
17
LOAD
15
CONTROL PANEL
POTENTIOMETER
36
88
MANUAL
34
DOSE RATE METER
54
33
DOSIMETER AMPLIFIER
AFC
57
35
59
MAGNET & MAGNET POWER SUPPY
MAGNETRON
19
TUNER
18
14
39
STEPPING MOTOR
38
STEPPING MOTOR DRIVER
73
74
STEPPING PULSE GENERATOR
37
91
94
41
12
GUN
25
MAIN PULSE TRANSFORMER
24
MODULATOR
23
TRIGGER PLUSE AMPLIFIER
22
MAIN TRIGGER GENERATOR
21
PULSE RATE SWITCH

FIG. 1

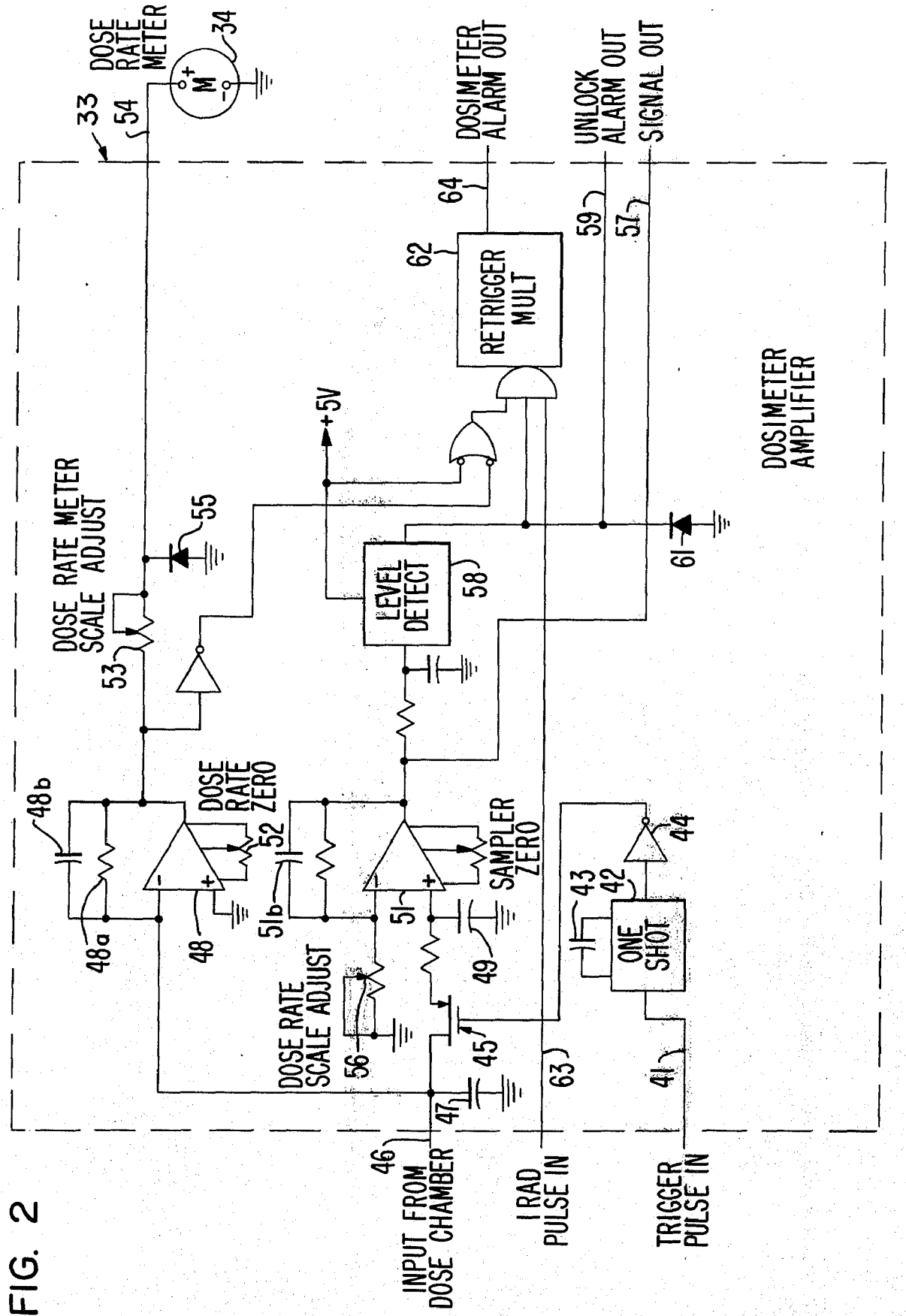

DOSE RATE METER
34
33
54
DOSIMETER ALARM OUT
UNLOCK ALARM OUT
SIGNAL OUT
64
62
59
57
RETRIGGER MULT
+5V
DOSIMETER AMPLIFIER
DOSE RATE METER SCALE ADJUST
55
53
LEVEL DETECT
58
61
48b
DOSE RATE ZERO
52
SAMPLER ZERO
44
43
42
ONE SHOT
48a
48
51b
51
49
DOSE RATE SCALE ADJUST
56
45
63
41
47
46
INPUT FROM DOSE CHAMBER
I RAD PULSE IN
TRIGGER PULSE IN

FIG. 2

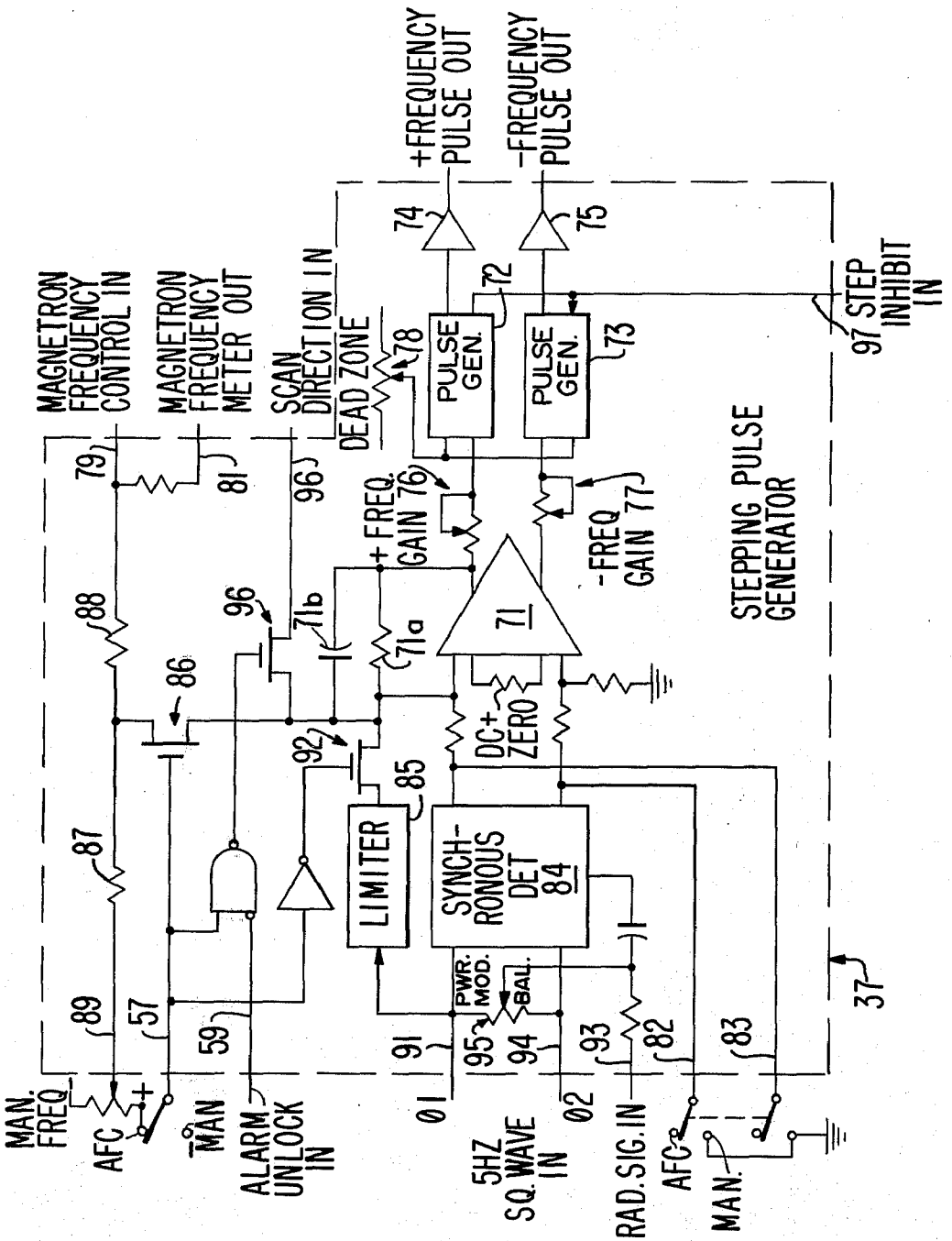

MAGNETRON FREQUENCY CONTROL IN
MAGNETRON FREQUENCY METER OUT
SCAN DIRECTION IN
DEAD ZONE
+FREQUENCY PULSE OUT
-FREQUENCY PULSE OUT
STEP INHIBIT IN
PULSE GEN.
PULSE GEN.
+ FREQ. GAIN
-FREQ GAIN
STEPPING PULSE GENERATOR
LIMITER
SYNCH-RONOUS DET
PWR. MOD.
BAL.
DC+ ZERO
MAN. FREQ
AFC
MAN
ALARM UNLOCK IN
5HZ SQ. WAVE IN
RAD. SIG. IN
AFC
MAN.

FIG. 3

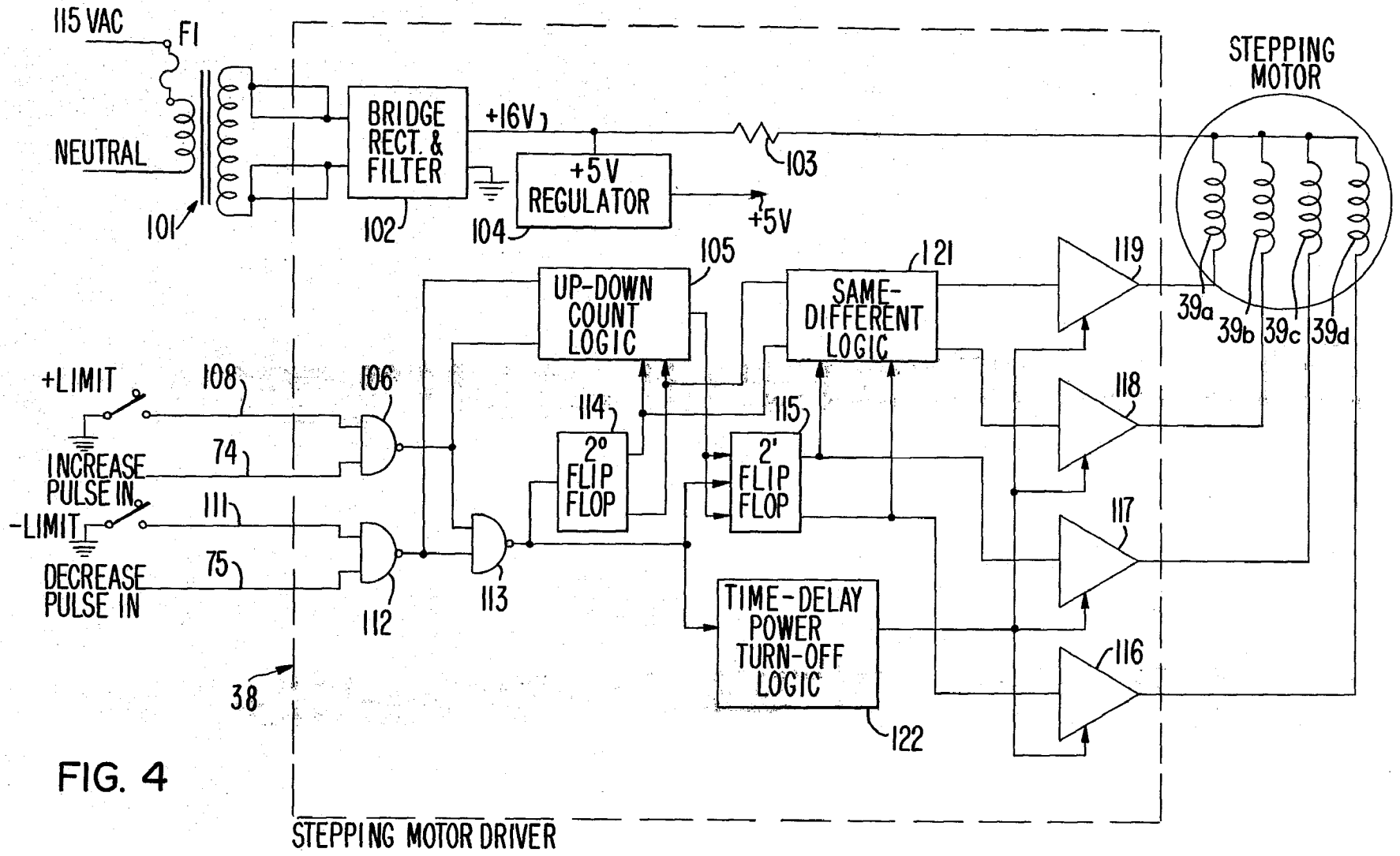

115 VAC
F1
NEUTRAL
101
BRIDGE RECT. & FILTER
102
+16V
103
+5V REGULATOR
104
+5V
STEPPING MOTOR
39a
39b
39c
39d
UP-DOWN COUNT LOGIC
105
SAME-DIFFERENT LOGIC
121
119
118
117
116
+LIMIT
108
106
INCREASE PULSE IN
74
-LIMIT
111
DECREASE PULSE IN
75
112
113
114
2° FLIP FLOP
115
2' FLIP FLOP
TIME-DELAY POWER TURN-OFF LOGIC
122
38
STEPPING MOTOR DRIVER

FIG. 4

AUTOMATIC FREQUENCY CONTROL SYSTEM FOR DRIVING A LINEAR ACCELERATOR

BACKGROUND OF INVENTION

Particle accelerators such as linear accelerators are used today in a number of different applications such as radio therapy, radiography and sterilization. In most of these applications the particle accelerator is used to generate X rays that are applied to the object.

It is very important that a constant dose rate output from the accelerator be achieved over both the short period of time, such as during a specific therapy treatment, as well as the long period of time such as day to day during successive treatments.

One of the biggest sources of possible variation in the output from an accelerator is the change in particle output amplitude resulting from a mismatch between the operating frequency of the accelerator and the driving frequency signal applied thereto. This mismatch can result from dimensional changes in the accelerator structure due to changes in the temperature of the structure or differential expansion in different parts of the accelerator structure thereby resulting in a change in its operational frequency.

In the past, efforts to maintain desired relationship between the driving frequency source and the accelerator have been to use a stabilization device such as a stabilizing frequency cavity which is physically attached and maintained in the environment of the accelerator and stabilizes the frequency of the source to the operational frequency of the accelerator. Changes in the dimensions of the accelerator causing a change in its operational frequency would usually also be accompanied by a change in the stabilization cavity so that the stabilization cavity would stabilize the driving signal source at the desired frequency for operation of the accelerator. However, it has never been possible to perfectly match the stabilization cavity to the accelerator structure and thereby keep the driver source tuned to the best operational frequency for the accelerator.

SUMMARY OF THE INVENTION

This invention relates to an automatic frequency control for maintaining the frequency of the accelerator driver source always tuned to the operational frequency of the accelerator.

In accordance with this invention method and apparatus are provided whereby the particle output amplitude from the accelerator is measured and the frequency of the driver source is maintained at a desired level to maximize the particle output amplitude.

The particle output amplitude is measured by a signal derived from an ionization chamber wherein current pulses are sampled to obtain an output signal representative of modulated particle (X-ray) pulses. This signal is amplified and applied through the automatic frequency control aspect of the system to a stepping pulse generator wherein a signal is added to minimize power modulation effects of the accelerator RF source and synchronously demodulated to produce a frequency error voltage and stepping pulses having rates which are proportional to this error voltage. The stepping pulses are directed to the drive of a stepping motor to step the tuner of the driver source to the point where particle amplitude is maximized.

In accordance with another aspect of this invention, the principle components of the system can also be used in a manual frequency mode wherein the desired frequency for the driver source is set and the stepping motor driven with stepping pulses until the difference between the desired setting and the frequency setting measured on the source is reduced to zero.

These and other features and advantages will become more apparent upon a perusal of the following specification taken in conjunction with the accompanying drawings wherein similar characters of reference refer to similar structures in each of the several views.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1 is a schematic block diagram of an accelerator control system in accordance with the present invention.

FIG. 2 is a block diagram of a dosimeter amplifier utilizable with this invention.

FIG. 3 is a block diagram of a stepping pulse generator utilizable with the present invention.

FIG. 4 is a block diagram of a stepping motor driver assembly utilizable with the present invention.

DETAILED DESCRIPTION OF A PREFERRED EMBODIMENT OF THE INVENTION

While it will be appreciated that the present invention has application to automatic frequency control in other applications such as with other particle generating systems, it is ideally suited to automatic frequency control of a linear accelerator system and thus will be described with reference thereto.

Referring now to the drawings with particular reference to FIG. 1, a linear accelerator **11** is schematically illustrated provided with an electron gun assembly **12** at one end for generating and directing a stream of electrons longitudinally of the accelerator and a target **13** such as of gold positioned at the opposite end for generation of X-rays upon bombardment by the accelerated stream of electrons. This stream of electrons is accelerated by energy exchange with a radio frequency wave which is introduced at an appropriate cavity of the accelerator **11** which takes the form of a coupled cavity structure.

The radio frequency energy is directed to the accelerator **11** from a source such as a magnetron or a klystron tube. In the present illustrative embodiment a magnetron **14** is provided with its output directed through a circulator **15** to the RF input window **16** of the accelerator **11.** An RF load **17** is also connected to the circulator **15** to absorb any reflected energy.

The magnetron **14** is provided with a tuner assembly **18** of any well-known type and an associated potentiometer **19** calibrated with the output frequency of the magnetron.

For establishing the pulsed electron beam in the accelerator and automatic frequency control of the system a pulse rate switch **21** is provided for selecting the desired pulse rates such as 120, 180, 240, 300 and 360 pulses per second (pps) as established in a main trigger generator **22.** Trigger pulses established in this generator **22** are amplified in a trigger pulse amplifier **23** and directed to a modulator **24** for modulation of the magnetron **14** and the accelerator gun **12** through a main pulse transformer **25.**

The X-ray intensity output of the accelerator is monitored in an ion chamber **31** having pairs of plates **30** and **32** and associated plates (not shown) connected to a dosimeter power supply **31'**. The X-rays passing through the dose chamber produce an ionization of the

air in the chamber and cause a charge to be collected on plates therein. A pulse current from one of the two plates **30** of the ionization chamber **31** is directed to a dosimeter amplifier **33** which filters and amplifies its current to display a dose rate on a dose rate meter **34** located on the front of the control console for the accelerator. The dosimeter amplifier **33** also samples the pulse current to obtain an output signal representative of the modulated X-ray pulses for use in the automatic frequency control (AFC) system.

A switch **35** is provided to switch between AFC operation and a manual operation system wherein a desired operational frequency is manually selected on a potentiometer **36** on the control panel for the accelerator.

Control of the magnetron frequency through the AFC or manual selection process is accomplished by connection of the output from switch **35** through a stepping pulse generator **37** which is connected to a stepping motor driver assembly **38** for drive of a stepping motor **39** connected to the magnetron tuner **18.**

In the manual mode of operation with switch **35** connecting potentiometer **36** to the stepping pulse generator **37,** an amplifier in the stepping pulse generator **37** is provided with an input which is the difference between the frequency setting of the magnetron potentiometer **19** and the desired operational frequency on the control panel potentiometer **36.** Stepping pulses are generated and directed to the stepping motor driver **38** and stepping motor **39** for movement of the magnetron tuner **18** until the difference of this input is reduced to zero at which point the magnetron is tuned to the desired frequency manually set on the control potentiometer **36.**

In the AFC mode, the stepping pulse generator **37** obtains a 5 Hz square wave signal from the main trigger pulse generator **22** to produce a sawtooth frequency modulation of the magnetron. The generator **37** also receives a return signal via the ion chamber **31** and dosimeter amplifier **33** representing the modulated X-ray pulse amplitude, adds a signal to minimize the power modulation effects of the magnetron, and synchronously demodulates the net signal to produce a frequency error input voltage to a dual output amplifier for driving the tuner stepping motor **39** through the stepping motor driver **38.** The resulting net signal in the stepping pulse generator **37** before demodulation has amplitude and polarity which are determined by the frequency modulation of the magnetron and the offset between the magnetron frequency and the resonant frequency of the accelerator guide, at which maximum X-rays are produced.

A total dose integrator **40** receives current from another plate **32** of the ionization chamber **31** and produces an output pulse each time that a charge equivalent to 1 rad of total dose has been accumulated. The dose integrator **40** is interlocked so that the 1 rad output pulses can be obtained only when X-rays are turned on. These output pulses go to the counter input of a dose decade counter display **40'** and to the dosimeter amplifier **33** as one of the inputs to the dosimeter alarm portion of the dosimeter amplifier **33.**

Referring now to FIG. **2** there is shown a schematic block circuit block diagram of the dosimeter amplifier **33.** Besides sampling the ionization chamber plate current to display dose rate and obtain a signal representative of the modulated X-ray pulses for use in the AFC system, an unlock alarm signal is generated if the X-ray output is too low, and this unlock alarm signal causes the AFC system to scan, looking for the right frequency. Additionally, a dosimeter alarm circuit compares the output of the dose rate circuit, the sampling circuit and the rate of rad pulses from the integrator **40.** If any of these latter three signals are below pre-set thresholds, due either to failures in the circuits, the cables, the chamber **31** or supply **31'**, a dosimeter alarm is initiated which turns the X-rays off.

With specific reference to FIG. **2,** whether X-rays are on or not, negative trigger pulses to be used for generating sampling pulses are present at input **41,** which are obtained from the main trigger pulse generator **22.** The frequency, from 120 to 360 pps, of these pulses is set by the pulse rate switch **21** on the control panel. These pulses trigger a one-shot multivibrator **42** which produces positive output pulses such as of 20 ns width in this one illustrative embodiment as determined by a timing capacitor **43,** and drives an inverting amplifier **44** to produce a negative going pulse of 15 volt amplitude. This pulse drives a sample and hold FET circuit **45** which receives, when X-rays are on, pulses of negative current flow through a coaxial line **46** from plate **32** in the ionization chamber in the X-ray beam. These current pulses produce negative voltage pulses on the input capacitor **47** which decay to ground potential due to the loading of an inverting operational amplifier circuit **48** input. The peak negative voltage on the input capacitor **47** is sampled and transferred to a holding capacitor **49** connected to the input of a non-inverting operational amplifier **51.**

Since the holding capacitor **49** is a small percentage of the input capacitor **47,** very little current flows, and after the first pulse the current through the FET switch **45** will depend only on the difference between the pulse being sampled and the previous pulse. Both operational amplifiers **48** and **51** are FET input amplifiers having extremely low bias current. Therefore, there is essentially no charge from the ionization chamber lost in the operational amplifier inputs, consequently all ionization chamber charge must flow through the input resistor and feedback resistor **48***a* of the inverting operational amplifier **48** where, with the aid of the filtering effect of a feedback capacitor **48***b*, the averaged output voltage is a faithful reproduction of the average dose rate.

A zero adjustment for this dose rate output voltage is provided by a potentiometer **52** in the operational amplifier circuit **48,** and a potentiometer **53** leading to an output **54** sets the average current to the dose rate meter **34** on the control console panel. A shunt diode **55** serves as a reverse voltage protection for the dose rate meter **34** during initial calibration and testing.

The sampled voltage held on the holding capacitor **49** is amplified by the non-inverting operational amplifier **51** and an operational amplifier input potentiometer **56** furnishes a gain adjustment. A small amount of filtering is provided by a feedback capacitor **51***b* so that the output is a faithful reproduction on a pulse-to-pulse basis of the charge collected by the ionization chamber and exists at the amplifier **51** output as a signal of approximately −9 volts average level. This signal leaves the dosimeter amplifier circuit **33** at output **57** for purposes of AFC tuning where the modulation riding on this signal is AC coupled to a synchronous detector in the stepping pulse generator **37.**

For providing low X-ray level and off frequency alarms the average level of the signal at the operational amplifier **51** output is filtered and is normally negative

enough to keep the output of a level detect circuit **58** high. This puts the output voltage at output **59** up to +5 volts representing no unlock alarm. When the X-ray pulse amplitude is reduced to approximately 70 percent of its normal level, the non-inverting operational amplitude **49** output rises to the point where it causes the level detect circuit **58** output to be clamped near ground potential by a diode **61** at its output. The unlock alarm voltage now near ground potential goes to the stepping pulse generator circuit **37** where it initiates a frequency scan when the switch **35** is in the AFC mode. When in the manual mode, this voltage has no effect on the frequency setting.

A retriggerable multivibrator **62** is provided, such as an integrated circuit, having the property that, if it is retriggered by an input pulse before its cycle recovery from a previous one, it begins a new pulse. At the lowest pulse rate settting of 120 pps and for normal X-ray output, one rad pulses from the total dose integrator which enter at input **63,** continuously cause retriggering at timed intervals which are approximately one-third of the 1.5 second pulse width as set by the pulse width setting network. This causes an output **64** to be continuously low representing no dosimeter alarm to the fault logic of the system. If the total dose integrator **40** fails to function, or if it delivers pulses at less than one-third its minimum rate, the dosimeter alarm output **64** will rise at the end of a 1.5 second interval and X-rays will be turned off. Normally the dosimeter rate input voltage to the multivibrator **62** logic is zero and the amplitude discrimination input is high. If either of these two voltages changes state, due either to the failure of the dose rate amplifier **48** circuit or the sampling amplifier **52** circuit, these new voltage levels into the retriggering multivibrator **62** input logic will inhibit the retriggering by the 1 rad pulses. A dosimeter alarm then results at output **64.**

As shown in FIG. **3** the stepping pulse generator circuit **37** contains a dual output operational amplifier **71** which drives two separate stepping pulse generators **72** and **73.** These generators **73** and **72** produce decrease and increase frequency pulses for the stepping motor driver assembly **38** which drives the stepping motor **39** to control the magnetron tuner **18** as described in greater detail below with reference to FIG. **4.** In the manual position of control **35** the amplifier **71** obtains an input which is the difference between the frequency setting, as measured on the magnetron tuner potentiometer **19,** and the desired frequency as set by the manual frequency potentiometer **36** on the control panel. Stepping pulses are generated until this difference is reduced to zero. In the AFC mode, the circuit **37** obtains a 5 Hz square wave signal from the main trigger pulse generator **22** which is used to produce a sawtooth frequency modulation of the magnetron **14.** The circuit receives a return signal on input **93** representing the modulated X-ray pulse amplitude from the dosimeter amplifier circuit **33,** adds a signal to this to minimize the power modulation effects of the magnetron, and synchronously demodulates the net signal to produce a frequency error input voltage to the dual output amplifier **71.** The stepping pulses have rates which are proportional to this error voltage. A separate unlock alarm input **59** will initiate a sawtooth frequency scan in the AFC mode if the X-ray amplitude is below approximately 70 percent of its normal level.

The dual input, dual output integrated circuit operational amplifier **71** has its corresponding inputs and outputs oppositely phased. A DC zero adjustment is provided. Frequency roll off and amplifier gain characteristics are accomplished by the shunt **71***a* and **71***b* network connected as feedback around the amplifier **71.** The output has a dynamic range of approximately −8 to +8 volts. When the plus frequency output signal is positive and increasing, it increases the charge rate of a unijunction transistor pulse circuit within the upper pulse generator **72** as shown in the block diagram causing an increase of increase frequency pulses at output **74.**

At the same time, the opposite amplifier output is equally negative and cuts the lower pulse generator **73** off which results in an absence of decrease frequency pulses at output **75.** The two circuits are similar and operate symmetrically and have plus frequency gain and minus frequency gain potentiometers **76** and **77** in their respective pulse circuit charge paths for factory adjustments. When the two operational amplifier outputs are equal in voltage, this voltage is not necessarily zero, and a dead zone adjustment **78** is therefore necessary to get a smooth cross over between the positive and negative pulse generators. The outputs **74** and **75** are positive going, 5 volt pulses, AC coupled into an external 180 ohm load in the stepping motor drive assembly **38.** The two pulse generators **72** and **73** are cross coupled to inhibit the charge rate of each other so that random noise at the output of the operational amplifier **71** will not cause simultaneous unijunction triggering in both pulse generators, which would result in random stepping. Both pulse generators **72** and **73** are inhibited by a −15 volt signal entering at input **97** during the first second after X-rays are turned on. After this one second delay, in which the high voltage is being run up in the modulator **24,** the pulse generators are released and frequency tuning can commence either manually or automatically.

As previously stated, the increase and decrease frequency pulses out of this circuit are decoded by the stepping motor driver assembly **38,** to drive the stepping motor **39** on the magnetron tuner **18.** This motor tunes the magnetron over a frequency range of approximately 1.5 gHz. The potentiometer **19** on this assembly is coupled to the motor to produce an analog indication of the position of the tuner within this range. The voltage from this potentiometer, which increases as the frequency increases, enters at input **79** and is brought out through output **81** to a frequency meter on the control panel.

When the AFC-control switch **35** on the control panel is in the manual position, inputs **82** and **83** are grounded, and a minus voltage input exists on input **57.** Inputs from a synchronous detector **84** to the operational amplifier **71** are therefore grounded. A limiter **85** and the scan direction inputs to the amplifier **71** are disconnected by the minus voltage inputs to their respective FET switch circuits. The only input remaining comes from the minus voltage actuated FET switch **86** connecting to the voltage averaging resistors **87** and **88** which exist between the manual frequency adjust potentiometer voltage at input **89** and the magnetron frequency control voltage entering at input **79.** Pulses are produced until the averaged voltage between the two inputs is reduced to zero, at which point the magnetron is tuned to the desired frequency as set by the manual frequency adjust potentiometer **36.**

In the AFC mode, input **57** is positive which disconnects the manual frequency control circuits and con-

nects the limiter **85** signal to the operational amplifier **71.** The synchronous detector **84** also becomes effective by having its outputs disconnected from ground. In the AFC mode the circuit **37** is used both to provide frequency modulation of the magnetron and to tune the magnetron for maximum X-ray output in response to a return signal which the card synchronously demodulates. The 5 Hz square wave modulating signal froom the main trigger pulse generator **22** entering at input **91** is limited and coupled through its FET switch **92** to the operational amplifier **71.** The amplifier partially integrates this signal to produce oppositely-phased approximate sawtooth voltages at its two outputs which respectively modulate the pulse rate generators, and consequently frequency modulating the magnetron.

A signal from a sample and hold amplifier of the dosimeter amplifier circuit enters at input **93.** This signal represents the pulse-to-pulse variation in X-ray amplitude. A 5 Hz square wave at inputs at **91** and **94** from the main trigger generator and whose amplitudes and polarities are adjustable by a power modulator balance potentiometer **95** is added to this signal to cancel X-ray amplitude modulation produced by power modulation of the magnetron. The resulting AC portion of the signal which is capacitance coupled to the synchronous detector **84,** has amplitude and polarity which are determined by the frequency modulation of the magnetron plus the offset between the magnetron frequency and the accelerator guide resonant frequency, at which maximum X-rays are produced. This signal will have zero amplitude if the frequency offset between magnetron and accelerator guide is zero. This signal is detected to produce a DC input to the operational amplifier **71** by the synchronous detector **84** whose gating signals are the oppositely phased **5** Hz square waves entering at inputs **91** and **94.** The DC input is amplified by the inverting and non-inverting gain alternately with the net resulting output being additive and representing either an increase or decrease frequency tuning signal. When the demodulated DC voltage is different from zero, stepping pulses are generated which tune the magnetron so as to produce maximum X-ray output, at which point the synchronously detected amplitude variations will be zero.

The unlock alarm signal at input **59** comes from the dosimeter amplifier circuit **33** and is normally +5 volts unless the X-ray amplitude is less than **70** percent of its normal value, in which case this voltage goes to ground potential. The ground state represents an unlock alarm which turns the scan direction FET switch **96** on and permits scan signal inputs to the operational amplifier which are sufficient to drive the amplifier to its positive or negative saturation limits depending from input **96** on the setting of a scan direction switch on the magnetron tuner assembly. This signal is strong enough to override any input signal entering the operation amplifier **71** from the synchronous detector **84.** Frequency is then scanned, and at the end of travel, the scan direction switch is toggled so that a scan in the reverse direction is initiated. One period of this sawtooth frequency scan takes approximately two seconds. As the magnetron frequency approaches the frequency at which maximum X-rays are generated, the unlock alarm signal will change state, open circuiting the scan signal path anad stopping the scan. The input signal from the synchronous detector **84** will then take over and the servo will achieve capture in the normal fashion. Should the peak X-ray level be less than 70 percent of normal for some reason, the unlock alarm input will not change state, and X-rays will be turned off within 1.5 seconds by the dosimeter alarm circuit on the dosimeter amplifier circuit **33.** Frequency scanning will continue until the time of X-ray turn off, at which point a negative voltage input at input **97** will inhibit the two stepping generators.

Carrying on from the stepping pulse generator **38** of FIG. 3 to the stepping motor drive of FIG. **4,** the stepping motor driver circuit accepts 115 VAC as a power input and generates +16 VDC for powering the stepping motor **39** and +5 VDC for powering the digital driving logic. Increase and decrease pulses enter on coaxial line inputs from the stepping pulse generator **37.** These pulses are counted and decoded by the digital logic so that the four windings **39***a–d* on the stepping motor **39** are energized in proper sequence.

The 115 VAC input is transformed in transformer **101** to 12.6 VAC which is full wave rectified and filtered at **102** to produce +16 VDC. A power resistor **103** drops this voltage to +8 VDC when the stepping motor **39** is operated in the normal manner. A regulator **104** for the power supply produces +5 volts for powering the circuits of the driver.

A positive increase pulse enters the card at input **74.** This line is normally held down to a voltage near ground potential. The input should be at least 3 volts in amplitude and greater than 30 micro-seconds duration to produce a step. A negative output pulse is produced which sets the up-down count logic **105** to the increase state. The increase pulse is inhibited from passing through a first gate **106** if the increase limit switch **107** is closed. This line at input **108** is normally pulled up to +5 volts, but is grounded when the limit switch is actuated. The closing of the limit switch **107** does not produce any extra steps. A similar channel for decrease input pulses and the decrease limit switch **109** enters the card at inputs **75** and **111** producing negative decrease pulses through gate **112.** These pulses set the up-down count logic **105** states to the opposite state. Both increase and decrease pulses produce through gate **113** positive pulse outputs each of which produces a toggling of a 2^0 flip-flop **114** on the trailing edge of the pulse. A 2^1 flip-flop **115** is toggled on every other pulse, as controlled by the up-down count logic **105,** so that the two flip-flops function as an up-down counter. The outputs from the 2^1 flip-flop **115** drive the current amplifying channels **116** and **117** with oppositely phased square wave signals having the frequency of one-quarter the input pulse repetition rate. The outputs of the 2^0 and 2^1 flip-flops **114** and **115** are decoded by the same-different logic **121** to drive the other two current amplifying channels **118** and **119** with oppositely phased square waves also having the frequency of one-quarter the input pulse repetition rate.

A time-delay power turn-off logic **122** removes power from all four motor windings when no pulses are being received. This circuit senses when the spacing between pulses becomes greater than several seconds and produces an inhibiting input to all four current amplifiers **116–119.**

The main trigger pulse generator **22** takes three different phases of 12.6 VAC as inputs, producing pulses at the zero crossings of each to form a set of 6 pulses per line cycle. Different combinations of these six pulses are selected by the pulse rate switch **21** on the control panel for pulse rates of 120, 180, 240, 300 or 360 pulses per second (pps) to trigger the main thyra-

tron in the modulator and to supply pulses to the sample pulse generators on a gun heater controller and to the dosimeter amplifiers circuit **33**. These pulses are inhibited when a magnetron single misfire alarm occurs. In addition, these pulses are used to derive a square wave 5 Hz signal for the stepping pulse frequency modulation and demodulation used for AFC mode magnetron tuning.

While the invention has been described with reference to the use of a stepping motor and a stepping motor drive, other means such as a DC motor driven by the frequency error voltage can be utilized.

In other applications magnetrons have been modulated either by voltage modulation of the magnetron or a probe in the output to which a modulating signal is applied for reflective modulation of the magnetron signal. Both of these techniques result in undesirable power modulations. Frequency modulation by modulation of the tuner in accordance with the present invention results in minimum power modulation.

In accordance with another aspect of the present invention, the magnetron can be frequency modulated by modulating the magnetron magnet. This can be accomplished by a modification of the magnetic field of a permanent magnet but is more easily accomplished when an electromagnet is used for the magnetron. As shown in phantom in FIG. **1**, the modulation signal can be directed from the main trigger generator to an electromagnet power supply for the magnetron magnet.

What is claimed is:

1. A particle accelerator system comprising:
an accelerator guide means for accelerating particles,
particle injection means for injecting particles into said guide means,
a source of radio frequency energy,
means for frequency modulating said radio frequency energy source,
means for introducing radio frequency energy from said source into said guide means for energy exchange with and acceleration of said particles,
motor means connected to said source for changing the output frequency of said source,
means connected to said motor means for producing a drive signal to drive said motor means and change said source frequency,
means for sensing the output amplitude of accelerated particles from said accelerator guide means including means measuring current pulses of the accelerated particles from said accelerator guide means, and
means connected to said sensing means and to said drive signal producing means to activate said drive signal producing means and drive said motor means until the sensed output amplitude is maximum, said activating means including means for synchronously demodulating a signal received from said sensing means.

2. The system of claim **1** wherein said sensing means includes an ionization chamber, a particle collection plate in the chamber and means for sampling particle current at said plate to obtain an output signal representative of the modulated particle pulses.

3. The system of claim **2** including
means for driving said motor means across the range of frequency change of said source
means responsive to said sensing means to initiate said driving means when the particle output amplitude falls below a preset level.

4. The system of claim **3** including a particle integrator means connected to said sensing means for delivering particle pulses upon integration of a particle charge of a predetermined value.

5. The system of claim **4** including means for turning off the particle injection means either upon failure of particle integration pulses or continued operation of said initiation means after drive of said motor means across said frequency range.

6. The system of claim **1** wherein:
said source means includes a magnet structure and said frequency changing means includes means for modulating said magnet.

7. In a particle accelerator system having an accelerator guide, a particle injector, means for introducing into the guide radio frequency energy from a tunable radio frequency source, the improvement for maintaining the source at the desired frequency for driving the accelerator comprising:
means for tuning the source across a range of frequency change of the source,
means for modulating the particle pulses of the accelerator,
means for sensing the particle output amplitude from the accelerator and generating a signal representative of the modulated particle pulses,
means for synchronously demodulating the representative signal to produce a frequency error voltage,
means responsive to said error voltage for changing the frequency of the source whereby said source is tuned for maximum particle output amplitude, and
means responsive to said sensing means to initiate said tuning means when the particle output amplitude falls below a preset level.

8. In the particle accelerator system of claim **7**:
the source comprising a magnetron with a mechanical tuner for changing the frequency thereof,
said modulating means including means for modulating said tuner, and
said frequency changing means including means for driving said tuner.

9. In the particle accelerator system of claim **7**:
the source means comprising a magnetron with an electromagnet and
said modulating means including means for modulating said electromagnet.

10. In the particle accelerator system of claim **7** particle integrator means connected to said sensing means for delivering particle pulses upon integration of a particle charge of a predetermined value.

11. In the particle accelerator system of claim **10** means for turning off the particle injector either upon failure of particle integration pulses or continued operation of said initiation means after drive of said tuning means across said frequency range.

12. In a particle accelerator system having an accelerator guide, a particle injector, means for introducing into the guide radio frequency energy from a tunable radio source, the improvement comprising:
means for modulating the particle pulses in the accelerator,
means for sensing the particle output amplitude from the accelerator and generating a signal representative of the modulated particle pulses,
means for tuning the source across a range of frequency changes of the source,
potentiometer means for following the operating frequency setting of the source,

means for synchronously demodulating the representative signal to produce a frequency error voltage,

means responsive to said error voltage for driving said tuning means until the source is operating at the desired frequency,

potentiometer means for setting the desired operating frequency of the source and following the operating frequency setting of the source,

switch means for connecting one of said sensing means and the potentiometer means to said tuning means for changing the source frequency to the desired frequency setting or the frequency for maximum particle output amplitude,

means responsive to said sensing means to initiate said tuning means when the switch means connects said sensing means to said changing means and the particle output amplitude falls below a preset level,

particle integrator means connected to said sensing means for delivering particle pulses upon integration of a particle change of a predetermined value, and

means for turning off the particle injector upon failure of particle integration pulses or continued operation of said initiation means after drive of said tuning means across said frequency range.

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