

CRACKLIKE DEFECTS DETECTION AND SIZING FROM CO-OCCURENCE MATRICES

MOYSAN J.- BENOIST P.

CEA Centre d'Etudes de Sacloy, 91 - Gif-sur-Yvette (FR). Dept. de  
Technologie des Matériaux

CORNELOUP G.

Institut Universitaire de Technologie, 13 - Aix-en-Provence (FR)

MAGNIN I.

Institut National des Sciences Appliquées, 69 - Villeurbanne (FR)

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**CRACKLIKE DEFECTS DETECTION AND SIZING  
FROM CO-OCCURRENCE MATRICES**

J.Moysan<sup>1</sup>, G.Corneloup<sup>2</sup>, I.Magnin<sup>3</sup>, P.Benoist<sup>1</sup>

- 1.Lab. de Contrôle par Ultrasons (STA/LCUS)- CEN Saclay FRANCE
- 2.Lab. de Contrôle Non Destructif - IUT Aix en Provence FRANCE
- 3.Lab. de Traitement du Signal et Ultrasons - INSA Lyon FRANCE

**ABSTRACT**

The inspection of austenitic welds used in nuclear field with ultrasounds poses problems in interpretation : strong grain noise makes difficult the detection of the crack top and the crack bottom. Since corresponding echoes enable the defect sizing, defect sizing also becomes difficult. The formation of 2D images(BSCAN), and their processing enable an increase in the effectiveness of testing. We present a segmentation method, based on co-occurrence matrix, which separates defects zones and noise zones. Examples of segmentation improvement applied to artificial defects are presented .

**I. INTRODUCTION**

A powerful data acquisition and imaging system is developed by the CEA's Advanced Technology Departement. This system called SPARTACUS enables us to elaborate specific image processings . The system creates ultrasonic images where grain noise is the background and defects echoes are the picture's objects. Our work is research on a detection algorithm based on image segmentation. The segmentation method uses a thresholding technique based on the co-occurrence matrix [1]. A threshold can be defined from co-occurrence matrix [2],[3], and thus the analysis of the co-occurrence matrix enables us to separate defects from grain noise. In a second time, defect sizing could be achieved through the analysis of the processed image.

**II. DATA ACQUISITION**

The segmentation method is tested on images of defects fabricated by electroerosion in stainless steel plates which comprise an austenitic weld. Immersion technique is employed. We use 45° longitudinal waves. The central frequency of the focused probe,  $f_c$ , is 2 Mhz and the sampling frequency,  $f_e$ , is 20 Mhz. The total waveform is recorded. On Fig.1 a BSCAN of a

crack in a weld is represented. On this image several echoes are noticeable (1)(2)(3)(4), plus a large amount of grain noise. With no weld, only echoes (1)(2) would be noticed.

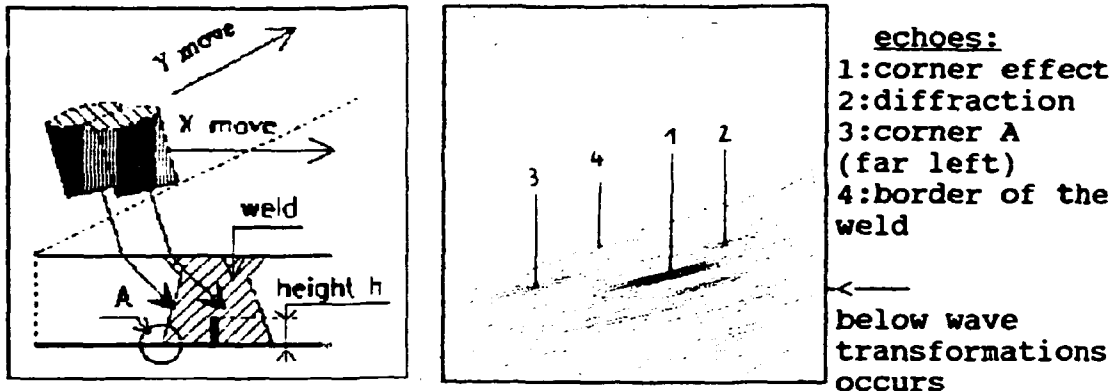


Fig.1. Ultrasonic testing system and BSCAN image.

### III. CO-OCCURRENCE MATRIX.

A pre-processing step is set down, the analytic signal [4] is employed in order to construct a simpler image.

#### III.1. Definition.

BSCAN image is described as a two dimensional function  $f$  defined over a discrete and finite domain  $D$ .  $D = X \times Y$ , a cartesian product of  $X$  which is the set of coordinates on the  $x$  axis and of  $Y$  which is the set of coordinates on the  $y$  axis,  $X = \{0, 1, \dots, M-1\}$ ,  $Y = \{0, 1, \dots, N-1\}$ . The function  $f$  takes its values in a discrete set  $e$  of  $L$  elements,  $f$  is then defined:

$$f: D \rightarrow e, f(x, y) \in e \quad (1)$$

$f(x, y)$  are pixel intensities, often described in gray levels. The co-occurrence matrix is a parametric function from  $e \times e$  to  $N$ . We note  $i$  and  $j$  the two variables of the co-occurrence matrix. The two parameters are the image  $f$  and a displacement vector  $d = [dx, dy]$ .

$$c: e \times e \rightarrow N \quad c(i, j, f, d) = |A_{ij}| \quad (2)$$

$|A_{ij}|$  is the cardinality of the set  $A_{ij}$  which is defined as:

$$A_{ij} = \{((x, y), (x', y')) \mid (x, y) \in D, (x', y') \in D \text{ and } (x', y') = t_d(x, y) \text{ and } f(x, y) = i \text{ and } f(x', y') = j\} \quad (3)$$

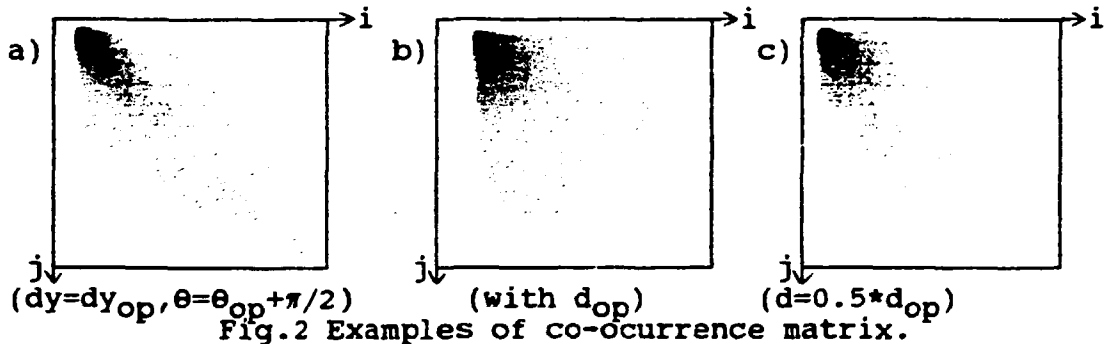
In this definition (3)  $t_d$  represents the translation of vector  $d$ . As indicated in (3)  $|A_{ij}|$  gives the number of co-occurrences in the image  $f$  of pairs of pixels, separated by a displacement  $d$ , which have respectively pixel intensity  $i$  and pixel intensity  $j$ . Symmetric co-occurrences matrices are obtained with the calculation of the coefficients  $c(i, j, f, -d)$ , we consider the coefficient  $C_{ij}$  defined the sum of  $c(i, j, f, d)$  and  $c(i, j, f, -d)$ .  $C_{ij}$  coefficients are normalized by dividing each coefficient by the total sum of  $C_{ij}$  coefficients.

### III.2. Calculation of matrices: the choice of vector d.

Numerous co-occurrence matrices can be calculated from the image  $f$  depending on the value of  $d$ . Two ultrasonic parameters help us to choose  $d$ . First, as explained in part II, a focused beam is used, so ultrasound path has an angle of  $45^\circ$  with the vertical in the plate reference system. This creates a optimal orientation in BSCAN image, we note  $\theta_{op}$  the corresponding angle in the image reference system. Second, the conversion of the central period of the transducer  $f_c$  in number of pixels on axis  $Y$  (temporal axis) gives a value called  $dy_{op}$ . With the previous notations (Cf.II.) we can write:

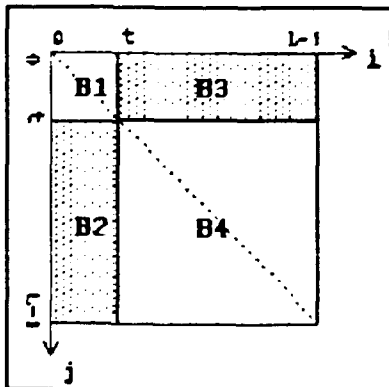
$$dy_{op} = f_e/f_c \quad (4) \quad \text{and} \quad dx_{op} = dy_{op} \cdot \tan(\theta_{op}) \quad (5)$$

The Fig.2 represents three normalized co-occurrence matrices displayed with 32 gray levels in logarithmic scale. Since the edges between grain noise and defects create off-diagonal elements in the co-occurrence matrix, the best discriminating matrix is the one for which off-diagonal entries are important. In Fig.2 the matrix which best fulfills this criterion is the one calculated with  $d_{op}=[dx_{op}, dy_{op}]$ .



### III.3. Threshold value selection.

Let  $t$  be a value for the searched threshold. The tested threshold  $t$  divides the co-occurrence matrix into four blocks of variable sizes  $B1(t), B2(t), B3(t), B4(t)$  as shown in Fig.3.



In the first block,  $i$  and  $j$  values are less than  $t$ , so the  $C_{ij}$  coefficients in this block represent all pairs of pixels whose pixel intensities are both less than  $t$ . In the same manner, the fourth block  $B4(t)$  represents all pairs of pixels whose pixel intensities are both greater than  $t$ . At last, in the second and in the third block, one of the two pixels has a pixel intensity less than  $t$  and the other one has a pixel intensity greater than  $t$ . The block  $B3(t)$  contains the information of the edges between noise and defect.

Fig.3. Matrix division.

The automatic threshold selection is based on this distribution of  $C_{ij}$  coefficients in co-occurrence matrix. A

function  $M(t)$  is calculated over a sub-division of the matrix. We have defined a function called Average Graylevel Variance Measure (AVGM) [5]. This function calculates the variance of the position of the  $C_{ij}$  coefficients in the third block. Thus the function is created to detect border region. With the Busyness [2] definition on block  $B_3(t)$  we have :

$$\text{Busy}(t) = \sum_{i=t}^{L-1} \sum_{j=0}^t C_{ij} \quad (6)$$

$$\text{AGVM}(t) = \frac{\sum_{i=0}^t \sum_{j=t+1}^{L-1} (i-\mu_i)^2 * (j-\mu_j)^2 * C_{ij}}{\text{Busy}(t)} \quad (7)$$

where  $\mu_i$  and  $\mu_j$  are means of  $i$  and  $j$  in block  $B_3(t)$ :

#### IV. CONCLUSION.

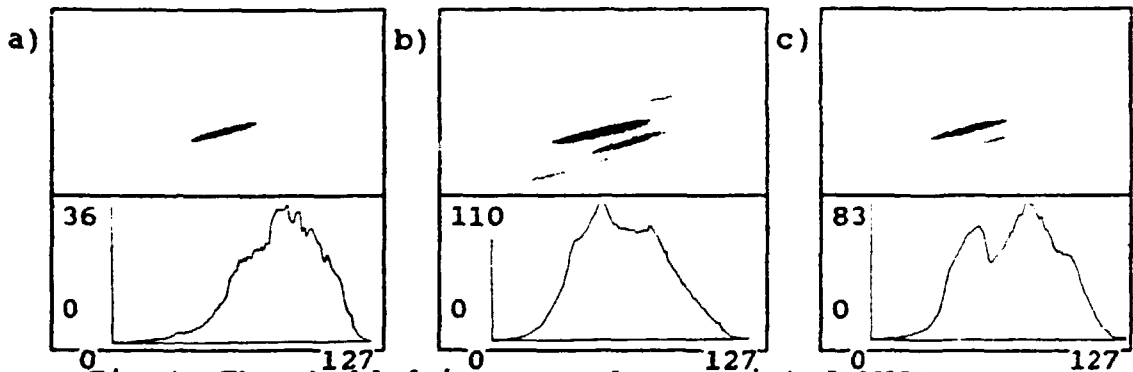


Fig.4. Thresholded images and associated AVGM curves.

Fig.4 shows three thresholded BSCAN with the algorithm applied on the image of Fig.1 for the same displacement vectors used in Fig.2. The second one, with  $d_{op}$ , enables us to successfully separate noise from the two defects echoes. In the first one, AVGM( $t$ ) is less discriminative and only the major echo is correctly obtained. A correct threshold is obtained from co-occurrence matrices analysis. This supposes a BSCAN image with at least a defect echo. Others applications can be developed for the analysis of BSCAN images in ultrasonic testing. These developments are currently studied in LCUS laboratory.

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