

## FEASIBILITY STUDIES OF USING THIN ENTRANCE WINDOW PHOTODIODES FOR CLINICAL ELECTRON BEAM DOSIMETRY

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### ABSTRACT

The response of the commercial XRA-24 PIN photodiode (5.76 mm<sup>2</sup> active area) for clinical electron beam dosimetry covering the range of 8-12 MeV was investigated. Within this energy range, the charge generated in the diode's sensitive volume is linearly dependent on the absorbed dose up to 320 cGy. However, charge sensitivity coefficients evidenced that the dose response of the diode is slightly dependent on the electron beam energy. Indeed, the diode's energy dependence was within 8.5% for 8-12MeV electron beams. On the other hand, it was also observed an excellent repeatability of these results with a variation coefficient (VC) lower than 0.4%, which is within the 1% tolerance limit recommended by the AAPM TG-62.

Furthermore, the agreement between the percentage depth dose profiles (PDD) gathered with the diode and the ionization chamber allowed achieving the electron beam quality within 1% of that obtained with the ionization chamber. Based on these results, the photodiode XRA-24 can be a reliable and inexpensive alternative for electron beams dosimetry.

### 1. INTRODUCTION

Silicon diodes have been widely employed in clinical photon beam dosimetry owe to a number of advantages over air-filled ionization chambers, commonly used for absolute and relative dose measurements. Among these advantages prevails the high sensitivity to ionizing radiation per unit volume of silicon which allows for design of compact-sized diodes. Such diodes are available with active area less than a few square millimeters and therefore with proper spatial resolution to be used in small field photons dosimetry [1-4]. Moreover, the progress in device design and fabrication technology has widened the range of applications of silicon diodes especially in those which require rather fine dead layer, such as, for example, soft X-ray detection and dosimetry [5-6].

In this context, several manufacturers have been involved in developing thin entrance window devices and one type of them, the PIN photodiode XRA-24 (Detection Technology Inc.) has proven to attain good performance in clinical photon beam dosimetry with almost negligible energy dependence. Taking into account this result and the features of these diodes, it seems quite feasible to employ them in electron dosimetry. In this context, the aim of this work was to study the XRA-24 diode's response for clinical electron beam dosimetry by investigating the following main dosimetry parameters: repeatability, charge versus dose response, energy dependence and percentage depth dose profile (PDD).

## 2. EXPERIMENTAL SETUP

In this work, the photodiode XRA-24, with active area of  $5.76 \text{ mm}^2$  ( $2.4 \text{ mm} \times 2.4 \text{ mm}$ ) was housed in a homemade polymer plastic probe covered by a  $100 \text{ mg/cm}^2$  black plastic layer. This probe was inserted in a depression at the center of a  $30 \text{ cm} \times 30 \text{ cm}$  polymethyl methacrylate (PMMA) plate with  $1 \text{ cm}$  thick, providing the diode's front side layer leveled with the surface of the plate. To perform the measurements, the  $n^+$  backside of the diode was kept grounded while the  $p^+$  front pad was connected in a short circuit mode to the input of an integrating electrometer (Standard Imaging model CDX 2000A).

The irradiations were performed with 8, 10 and 12 MeV electron beams from a Siemens Energy Mid Primus linear accelerator coupled to an electron cone applicator of  $10 \text{ cm} \times 10 \text{ cm}$ . Unless otherwise stated, during all measurements the diode was held between PMMA plates, placed at the reference depth and centered in a radiation field of  $10 \text{ cm} \times 10 \text{ cm}$ , with the source-to-surface distance (SSD) kept at  $100 \text{ cm}$ . For each of electron beam energies, the plastic reference depth was obtained from the water reference depth in accordance with IAEA/TRS-398 recommendations [7].

Firstly, the response repeatability of the diode was investigated for all electron beam energies. For each one, ten measurements were consecutively registered for the same radiation dose of  $100 \text{ cGy}$ , just switching on and off the electron beam. The repeatability performance was analyzed based on the variation coefficients (VC), obtained by the ratio between the standard deviation (SD) and the average reading.

To achieve the dose-response curve of the XRA-24 diode, given by the charge as a function of the absorbed dose, five consecutive measurements were carried out for each monitor unit value covering the range of 5 to  $320 \text{ cGy}$ . The absolute dose measurements were carried out using a calibrated parallel plate ionization chamber (Markus PTW 30013) coupled to an electrometer. The absorbed dose to water was calculated according to the International Atomic Energy Agency's absolute dosimetry protocol (Technical Reports Series 381), by applying appropriate correction factors for a beam quality and environment [8].

The dose-response curves were gathered for 8, 10 and 12 MeV electron beams and apart from the linearity analysis, the sensitivity coefficients ( $\text{nC/cGy}$ ) of the diode were obtained for each of electron beam energies. The diode's sensitivity dependence on the electron beam energy was also studied.

The percentage of depth dose (PDD) profiles of 8, 10 and 12 MeV electron beams were carried out in a PMMA phantom by changing the depth of the diode from 0 (phantom

surface) to 50 mm with PMMA plates, with SSD kept at 100 cm. For each position, two measurements were performed with a constant dose of 100 cGy. To obtain the PDD profiles, the dose measured at each depth was divided by that measured at the maximum dose depth and multiplied by 100. The experimental results gathered with the photodiode were compared with those obtained with the ionization chamber (Markus PTW 30013), measured in the water phantom. The PMMA thickness was converted to water thickness following IAEA/TRS-398 [7] recommendations. To give more substance to this comparison, values of mean energy of the electrons at the phantom surface ( $E_0$ ), the practical range ( $R_p$ ) and the half-value depth ( $R_{50}$ ) were obtained from the PDD curves of the diode and ionization chamber as well.

In all measurements, the combined uncertainties of the results were calculated with the well-known error propagation formula taking into account the diode's reading uncertainty, the accelerator's stability, both resolution and stability of the electrometer.

### 3. RESULTS AND DISCUSSIONS

#### 3.1. Repeatability

The average of ten consecutive measurements gathered at 100 cGy for 8, 10 and 12 MeV electron beams, with both correspondent standard deviation (SD) and variation coefficient (VC) are shown in Table 1. As can be seen, the VC values lower than 0.2%, fulfil the requirements of the AAPM protocol TG-62 [9], which recommends repeatability better than 1% for diodes used as dosimeters. These results are similar to those ( $VC < 0.5\%$ ) obtained with the diode of Scanditronix [10] and reported by Soriani et al. (2003). The response repeatability of the photodiode XRA-24 is better than that obtained with the photodiode BPW-34 employed in electron dosimetry [11].

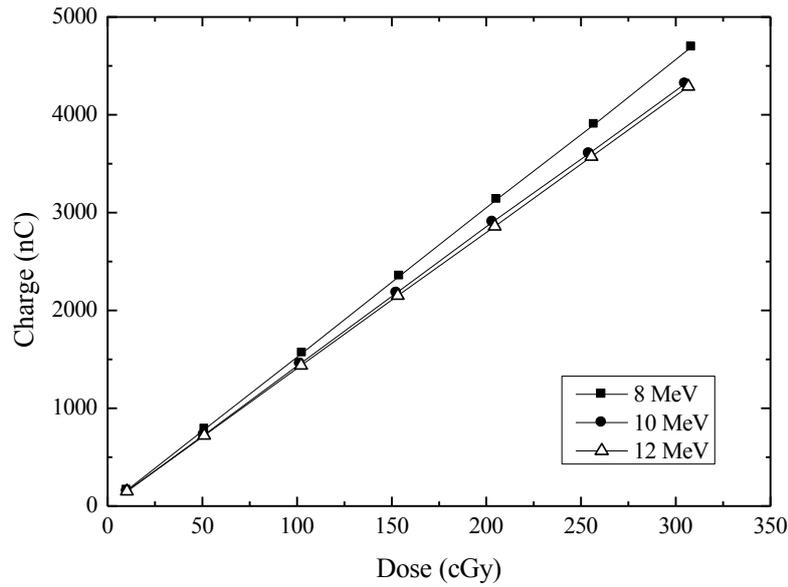
**Table 1: Mean reading of the diode, at 100 cGy, with the standard deviation (SD) and variation coefficient (VC) for 8, 10 and 12 MeV electron beams.**

Energy (MeV)	$\bar{M}_{Diode}$ (nC)	SD (nC)	VC (%)
8	1565.34	1.80	0.11
10	1454.00	2.13	0.15
12	1438.90	2.02	0.14

#### 3.2. Dose-Response and Energy Dependence

Figure 1 shows the charge generated in the diode as a function of the absorbed doses covering the range of 5–320 cGy. Each point corresponds to the mean value of five consecutive measurements carried out with the photodiode. The combined uncertainties associated with each value are lower than 0.8% for  $k=2$ .

As shown in Figure 1, the dose-response curves for all electron beam energies are quite linear (data fitting  $R^2$  coefficient higher than 0.99958) with charge sensitivity coefficients (nC/cGy), obtained from the angular coefficient of each dose-response curve, presented in Table 2.



**Figure 1: Dose-response curves of the diode for 8, 10 and 12 MeV electron beam energy.**

**Table 2: Charge Sensitivity coefficients of the XRA-24 photodiode for 8, 10 and 12 MeV electron beam.**

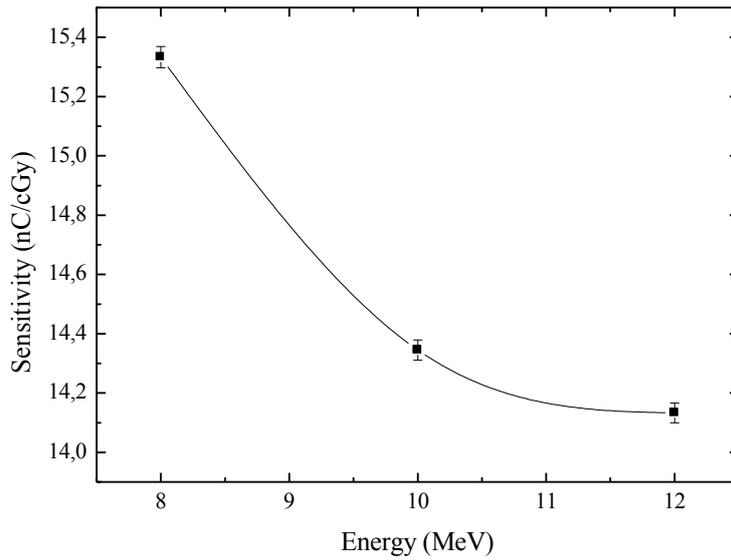
Energy (MeV)	Sensitivity Coefficient (nC/cGy)
8	15.33 ± 0.04
10	14.34 ± 0.03
12	14.13 ± 0.03

The variation of these sensitivity coefficients shows the dependence of the XRA-24 response on the electron beam energy. It is evidenced in Figure 2, where the charge sensitivity of 8 MeV electron beam is almost 8.5% higher than that obtained for 12 MeV electron beam. This energy dependence might be due to the difference of the deposited energy in the diode's sensitive volume by 8 and 12 MeV electron beams.

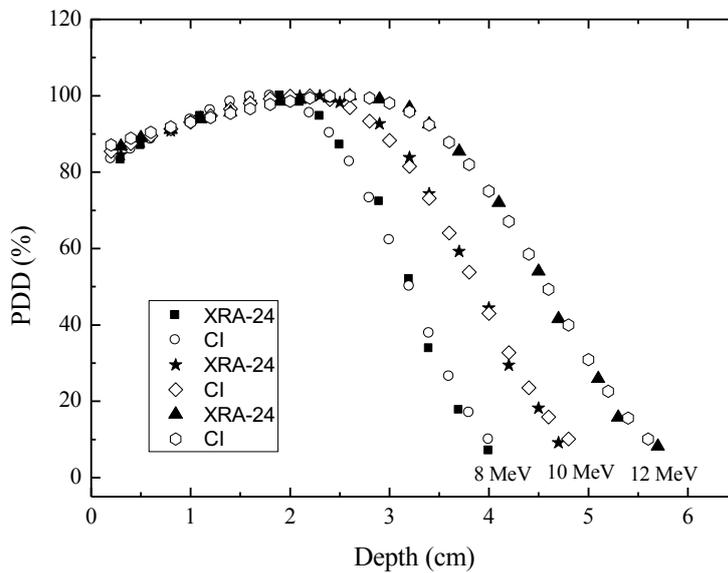
### 3.3. Percentage depth dose (PDD) profile

Figure 3 shows the percentage depth dose (PDD) curves carried out with the photodiode XRA-24 together with those obtained with the ionization chamber for 8, 10 and 12 MeV electron beam energies. For each of electron energies, the comparison of both dosimeters shows good agreement for PDD values higher than 25%. However, in the lower PDD region the response of the photodiode is 10% lower than that obtained with the ionization chamber. The mean energy of the electrons at the phantom surface ( $E_0$ ), the practical range ( $R_p$ ) and the half-value depth ( $R_{50}$ ) were also estimated from Figure 3. The value of  $E_0$  was obtained through the relationship obtained by the IAEA/TRS 381 [8]

$$E_0 = 0.656 + 2.059 R_{50} + 0.022 (R_{50})^2 \quad (1)$$



**Figure 2: Charge sensitivity coefficients of XRA-24 diode as a function of electron beam energies. The spline line is just a guide to the eyes.**



**Figure 3: Comparison between percentage depth dose (PDD) in water for 8, 10 and 12 MeV electron beam measured with XR-24 and ionization chamber Markus PTW 30013.**

The results of the mean energy of the electrons at the phantom surface ( $E_0$ ), the practical range ( $R_p$ ) and the half-value depth ( $R_{50}$ ), gathered from Figure 3, are presented in Table 3. The results obtained with the diode and the ionization chamber agreed within 2% which is comparable with the uncertainty values.

**Table 3: Mean energy of the electrons at the phantom surface ( $E_0$ ), the practical range ( $R_p$ ) and the half-value depth ( $R_{50}$ ) obtained with the XRA 24 and ionization chamber for electron beams of 8, 10 and 12 MeV.**

Nominal Beam Energy  E (MeV)	Photodiode –XRA-24			Ionization Chamber Markus PTW 30013		
	$\bar{E}_0$ (MeV)	$R_{50}$ (cm)	$R_p$ (cm)	$\bar{E}_0$ (MeV)	$R_{50}$ (cm)	$R_p$ (cm)
8	7.47	3.2	4.0	7.47	3.2	4.1
10	8.91	3.85	4.81	8.95	3.87	4.89
12	10.41	4.52	5.62	10.57	4.59	5.72

#### 4. CONCLUSIONS

The response of a PIN photodiode XRA-24 for clinical electron beam dosimetry was investigated in the energy range of 8-12 MeV energy. The results obtained with the diode operating in a photovoltaic model, evidenced that the charge generated in its sensitive volume increases linearly with the absorbed dose up to 320 cGy. It was also observed an excellent repeatability of these results with a variation coefficient (VC) lower than 0.4% and, therefore, within AAPM TG-62 Report 87 recommendations.

Despite of these good results, charge sensitivity coefficients evidenced that the dose response of the diode is slightly dependent on the electron beam energy. Indeed, the diode's energy dependence was within 8.5% for 8-12MeV electron beams. Furthermore, the agreement between the percentage depth dose profiles (PDD) gathered with the diode and the ionization chamber allowed achieving the electron beam quality within 1% of that obtained with the ionization chamber.

Based on these results, the photodiode XRA-24 can be a reliable and inexpensive alternative for electron beams dosimetry. Furthermore, it seems that this diode might be used for in vivo dosimetry as well as in small radiation field applications.

#### ACKNOWLEDGMENTS

The authors would like to acknowledge the financial support received from the Brazilian National Research Council (CNPq) and the Santa Casa de Misericórdia de Itabuna-Bahia.

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